



Angelo La Rosa<sup>1</sup>, Carol Lu<sup>1</sup>, Jason Boileau<sup>1</sup>, MacKenzie "Mac" Bradbeer<sup>1</sup>, Zain Syed<sup>1</sup> Olivia Burnsed, PhD<sup>1</sup>, Matthew Halanski, MD<sup>2</sup>, Cameron Jeffers<sup>3</sup> <sup>1</sup>School of Biological and Health Systems Engineering - Arizona State University, <sup>2</sup>Phoenix Children's Hospital, <sup>3</sup>University of Arizona

# **Clinical Need**



- **G**–**9 million** people in the U.S. experience scoliosis or spinal **deformities** due to growth plate disturbances [1].
- □ 38,000+ spinal fusion surgeries are performed annually to treat severe cases [1].
- $\Box$  15–30% of pediatric bone injuries involve growth plate fractures [2].
- Current implants use **rigid** fixation, which is non-ideal for growing bone. Rigid systems can lead to:
  - Stunted or uneven bone growth
  - > Delayed or impaired recovery
  - Poor compatibility with soft tissue in joints

Works Cited

**Device Concept** 

The BioSpring is a millimeter-scale force-modulating polymer spring designed to enhance structural elasticity in existing orthopedic platforms to build implants that grow with the patient.

Healthy Curvature Spinal Deformity



Fig 1. Curvature & Growth Plate Pinching in Spinal Deformities [3].





# **Specifications + Material Selections**

<b>Needs/Metrics</b>	Value
Young's Modulus	50-250 MPa
Load Withstood	35 N
Elastic Compressible Range	1-2 mm
Max Diametric Change at 8N	< 50%
Cell Viability	>95%
Swelling Ratio	Match or Less than Control
Max Force Generation	Match Control (7-9N)
Shear + Torsional Stress	Less than Control
Manufacturing Cost	Less than Control



**Fig 3. Material Selection Process via Ansys Granta** EduPack. TPU 20% Barium Sulfate hit the desired yield strength metrics with 98% similarity. Soft polymers were selected due to similar mechanical properties with a larger range of compressibility.

**Selected Polymers:** Thermoplastic Polyurethane (TPU)

**D**Polydimethylsiloxane (**PDMS**) Liquid Silicone Elastomer (LSE)

# **BioSpring: Small-Scale Orthopedic Implantables**











 Material Conditions Dimensional Combinations Total Unique

Experimental Groups

# Test Systems + Results



force-extension behaviors that fell between those of the two stainless steel controls and comparable Young's moduli, demonstrating suitable stiffness for dynamic orthopedic loading, while improving on the controls by having a smooth, predictable force response across a longer range of compression, and less slippage. All materials showed diametric deformation within the limits of the screw hole, showing structural compatibility.

Sample Type



**2** Swelling Ratio Testing dry weight SC1 SC2 PDMS 1mL cDMEM 10% 8 FBS/1% pen strep dry weight TPU-1 TPU-.5 LSE all others wet weight **Fig 5: Swelling ratios of various Polymer Swelling Ratios** polymer compositions tested for the BioSpring component. All % 30-24-18-12 materials except TPU with 50% infill showed a statistically significant reduction in swelling

compared to the stainless-steel controls (which had varying geometries), indicating their suitability as low-swelling alternatives for implant integration.



# **Prototyping + Experimental Design**

Material Characterization – How do the materials behave under mechanical stress?

1 Mechanical Compression Testing

**Implantable Feasibility** – How do the materials react to the conditions of the body?

2 Swelling Ratio Testing

3 Cell Viability Testing

**Device Validation** – Can the prototype produce an effective force in the final device?

4 Integrated Device Testing

Stress–Strain Comparison Across Materials (±1 SD shaded)

## **3** Cell Viability Testing







Fig 6: LSE Sample #2 after 96-hour growth period. Image contrast edited for increased cell visibility. Qualitative analysis shows cell proliferation across the stainless-steel control and all polymer samples. Subsequent reruns performed on LSE and PDMS samples over 24-hour period yielded similar results. Future experiments will involve Trypan blue staining with hemocytometers to quantify precise live/dead cell ratios.





**Fig 7: Validation testing.** Distribution (n=20) of remaining three experimental groups against control (C) in target range (7-9N). Kruskal-Wallis analysis confirmed significance between groups, post-hoc tests using Holm's method revealed statistical significance shown between Control and LSE 2x4 (\*p=0.0039). C vs LSE 2x3, p = 0.6941 and C vs LSE 3x3, p = 0.3514. LSE 2x3 and 3x3 were **not** statistically different from each other or C, indicating successful fit of target range and need for further testing.



We extend our thanks to Dr. Olivia Burnsed, Dr. Matthew Halanski, Cameron Jeffers, Dr. Bradley Greger, Dr. Brent Vernon, and Michael Sobrado for their guidance, trust, and support with the BioSpring project.



SBHSE School of **Biological** and Health Systems Engineering

# **Design Validation**



## **Final Design + Moving Forward**

- □ Next steps should include investigating
- LSE 2x3mm and 3x3mm with larger sample sizes.
- We recommend looking into medical-grade manufacturing practices for implantable devices, testing LSE's medical-grade counterpart (medical rubber), and exploring other manufacturing process to decrease dimensional tolerance (injection molding).
- As a component for implantable orthopedic devices, the BioSpring would be classified as a Class III Biomedical Device and will adhere to the necessary regulations and requirements.

# Acknowledgements

Fire A. Fulton Schools of Engineering **Arizona State University**